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# A Note on Population Analysis of Dissolution-Absorption Models Using the Inverse Gaussian Function

Jian Wang, PhD, Michael Weiss, PhD, and David Z. D'Argenio, PhD

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*Because conventional absorption models often fail to describe plasma concentration–time profiles following oral administration, empirical input functions such as the inverse Gaussian function have been successfully used. The purpose of this note is to extend this model by adding a first-order absorption process and to demonstrate the application of population analysis using maximum likelihood estimation via the EM algorithm (implemented in ADAPT 5). In one example, the analysis of bioavailability data of an extended-release formulation, as well as the mean dissolution times estimated in vivo and in vitro with the use of the inverse Gaussian function, is well in accordance,*

*suggesting that the inverse Gaussian function indeed accounts for the in vivo dissolution process. In the other example, the kinetics of trapidil in patients with liver disease, the absorption/dissolution parameters are characterized by a high interindividual variability. Adding a first-order absorption process to the inverse Gaussian function improved the fit in both cases.*

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**M**odeling the process of drug input to the systemic circulation is of central importance for fitting plasma concentration–time data following oral administration. In some cases, simple models (eg, first-order absorption) may be sufficient. The popular first-order absorption model, however, implies the unrealistic assumption that the maximum absorption rate is achieved instantaneously. Thus, more flexible descriptions of the drug input process (comprising dissolution and absorption) are often required. To address this problem, both non-parametric deconvolution methods (for review, see Verotta<sup>1</sup>) as well as parametric modeling approaches (for review, see Zhou<sup>2</sup>) have been proposed. After one of us<sup>3</sup> proposed the inverse Gaussian (IG) function as

a flexible empirical input function, it has been used to describe drug input for various extravascular administration routes.<sup>4–8</sup> Because the IG distribution has been found to be a suitable model for in vitro dissolution profiles,<sup>9</sup> its usefulness for oral extended-release formulations<sup>3,7</sup> is not surprising. It may be of interest to note that the IG is the first passage time distribution of a random walk with drift (first suggested by Schrödinger<sup>10</sup> in 1915) and the solution of the convection-dispersion equation for pharmacokinetically relevant boundary conditions.<sup>11</sup> The IG function has also been widely used to model the transit of drugs through organs and organ systems.<sup>12,13</sup>

The purpose of this note is 2-fold: (1) to illustrate the implementation of an IG input function in a compartmental disposition model for a population analysis of plasma concentration–time data following intravenous and oral data drug administration using ADAPT and (2) to extend the input model by adding a first-order absorption process to the IG function. The models presented are incorporated as part of the distributed library of the ADAPT software (Version 5) for pharmacokinetic/pharmacodynamic systems analysis.

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## METHODS

### Input Models

It is assumed that the plasma drug concentration following an oral administration of drug can be decomposed into an independent input process (representing the dissolution and absorption process) followed by the disposition process. The following single inverse Gaussian function can be used to model the complete input process.

$$f_i(t) = D \cdot F \sqrt{\frac{MIT}{2\pi CV_i^2 t^3}} \exp\left[-\frac{(t - MIT)^2}{2CV_i^2 MIT t}\right], \quad (1)$$

where  $MIT$  represents the mean input time and  $CV_i^2$  is a normalized variance ( $CV_i$  is the standard deviation of the density function  $f_i(t) / (D \cdot F)$  divided by  $MIT$ , ie, the relative dispersion of input times). The factor  $F$  is the bioavailability of the orally administered dose  $D$ . One can also calculate the model of the inverse Gaussian density as follows:

$$t_{i,max} = MIT \left( \sqrt{1 + \frac{9}{4} CV_i^4 - \frac{3}{2} CV_i^2} \right), \quad (2)$$

which is the time the input function achieves its maximum value (see Weiss<sup>3</sup>). As a single measure,  $t_{i,max}$  provides useful information about the input process.

Alternatively, the input process can itself be decomposed into an independent dissolution (or gastrointestinal transit time) component followed by an absorption component. Such a dissolution-absorption process can be modeled using an inverse Gaussian function to describe the drug's dissolution/transit (using the parameters  $MDT$  and  $CV_D$ ) followed by a first-order absorption model (with rate constant  $k_a = 1/MAT$ ). In this case, the mean input time is the sum,  $MIT = MDT + MAT$ .

### Study Designs and Data

In the first example, data from a previously described bioavailability study<sup>3</sup> of an undisclosed oral extended-release product are used to illustrate the method. Briefly, 10 subjects received both the oral and intravenous administration of the compound at the same dose in a crossover design. A total of 19 (oral) and 24 (intravenous [IV]) plasma concentrations were

collected between 5 minutes and 32 hours (1920 minutes) after the drug administration.

The second example involves the anti-ischemic drug trapidil. In this study, 12 patients with chronic liver disease were administered 100 mg of trapidil as a single intravenous bolus and 200 mg of trapidil as an oral dosage (Rocornal dragees 100 mg) in a crossover design. The intravenous data were published previously.<sup>14</sup> For the intravenous administration, 17 plasma samples were obtained between 5 and 420 minutes after injection, whereas 17 samples were taken between 15 and 480 minutes after oral administration.

### Population Modeling

Intravenous plasma concentration-time data were analyzed via population modeling using 1-, 2-, and 3-compartment linear models. Model selection was based on the Akaike information criterion (AIC). Population analysis was performed using maximum likelihood (ML) estimation (no linearizing approximations) via the EM algorithm as proposed by Schumitzky<sup>15</sup> and fully developed by Walker.<sup>16</sup> A program (MLEM) implementing this approach is available in the general pharmacokinetic/pharmacodynamic (PK/PD) systems analysis software ADAPT.<sup>17</sup> In addition to calculating the ML estimates for the population mean and covariance (intersubject variability), estimates for the individual subject parameters (conditional means) are also available.

Population analyses of the oral plasma concentration-time data were conducted using each of the 2 input models described previously: the single IG model of equation (1) (IG model) and the IG dissolution/transit plus first-order absorption process (IG/MAT model). For each analysis, the disposition model parameters for each subject were fixed at their conditional mean values determined from the intravenous population analysis (sequential analysis). As with the intravenous analyses, a lognormal population parameter model was assumed along with a proportional output error variance model.

## RESULTS

### Extended-Release Example

Based on the population modeling of the intravenous plasma concentration-time data, a 3-compartment disposition model was selected, as also found by the 3-exponential model fit reported by Weiss.<sup>3</sup> The

**Table I** Comparison of the Population Analysis of Oral Data for the Extended-Release Dosage Form Using the 2 Different Input Models

	IG/MAT Model			IG Model	
	Population Mean	Population SD		Population Mean	Population SD
$F$ , %	69.9	9.22	$F$ , %	69.8	9.10
$MDT$ , min	318	115	$MIT$ , min	332	77.7
$MAT$ , min	33.9	14.4			
$CV_D^2$	1.93	0.369	$CV_I^2$	1.22	0.178
$t_{D,max}$	53.4	19.8	$t_{I,max}$	84.8	19.7
AIC	1954			1970	

IG, inverse Gaussian; AIC, Akaike information criterion.

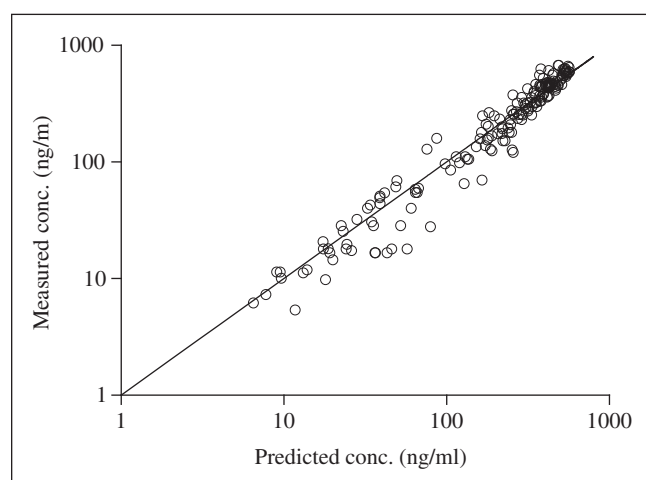


Figure 1. The measured oral (O) plasma concentration-time data of the extended-release drug versus their predicted values based on each subject's parameter estimates (conditional means) from the IG/MAT model.

results of the population analysis of the oral plasma concentration-time data are presented in Table I for the IG model and the IG/MAT model. The latter led to a smaller AIC value, with approximately 90% of the mean input time attributed to the dissolution process (see Discussion). The IG/MAT model results in a larger estimated maximum input rate than does the IG model. In Figure 1, the measured oral plasma concentration-time data are shown versus their predicted values based on the conditional mean estimates for each subject's parameters for the IG/MAT model. Figure 2 shows the predicted and observed intravenous and oral plasma concentration-time data for 2 subjects representing the largest and smallest values of  $MDT$ , along with the corresponding dissolution rate functions from the IG component of the input process.

An IG distribution function (ie,  $F_I(t) = \int_0^t f_I(\tau) d\tau / (D \cdot F)$ ) was also fitted to in vitro dissolution data of this extended-release formulation (population analysis of 12 dissolution profiles), which resulted in a mean  $MDT = 302$  min (SD = 39 min) and a relative dispersion  $CV_D^2 = 3.72$  (SD = 0.47). Figure 3 shows the measured data versus their predicted values obtained by the population fit of the dissolution data together with a representative dissolution profile.

### Trapidil Example

In accordance with the previous 2-exponential fit,<sup>14</sup> a 2-compartment disposition model was selected to describe the trapidil intravenous plasma concentration-time data based on the population analysis (results not shown). The population analysis results using the IG and IG/MAT model to fit the oral trapidil data are presented in Table II, with the IG/MAT model resulting in a lower AIC value. The predicted and observed intravenous and oral plasma concentration-time data for 2 subjects representing the largest and smallest values of  $MDT$  are shown in Figure 4, together with the predicted dissolution/transit rate functions.

### DISCUSSION

As summarized in Table I, the extended-release example data were best described by an input model that included a dissolution component modeled as an inverse Gaussian followed by a first-order absorption process. The modeling results indicate that approximately 90% of the mean input time is due to the dissolution process, with 10% due to the absorption process. Simultaneous population analysis was also performed by fitting both the  $C_{po}$  and  $C_{iv}$  data together (results not shown). The parameter estimates

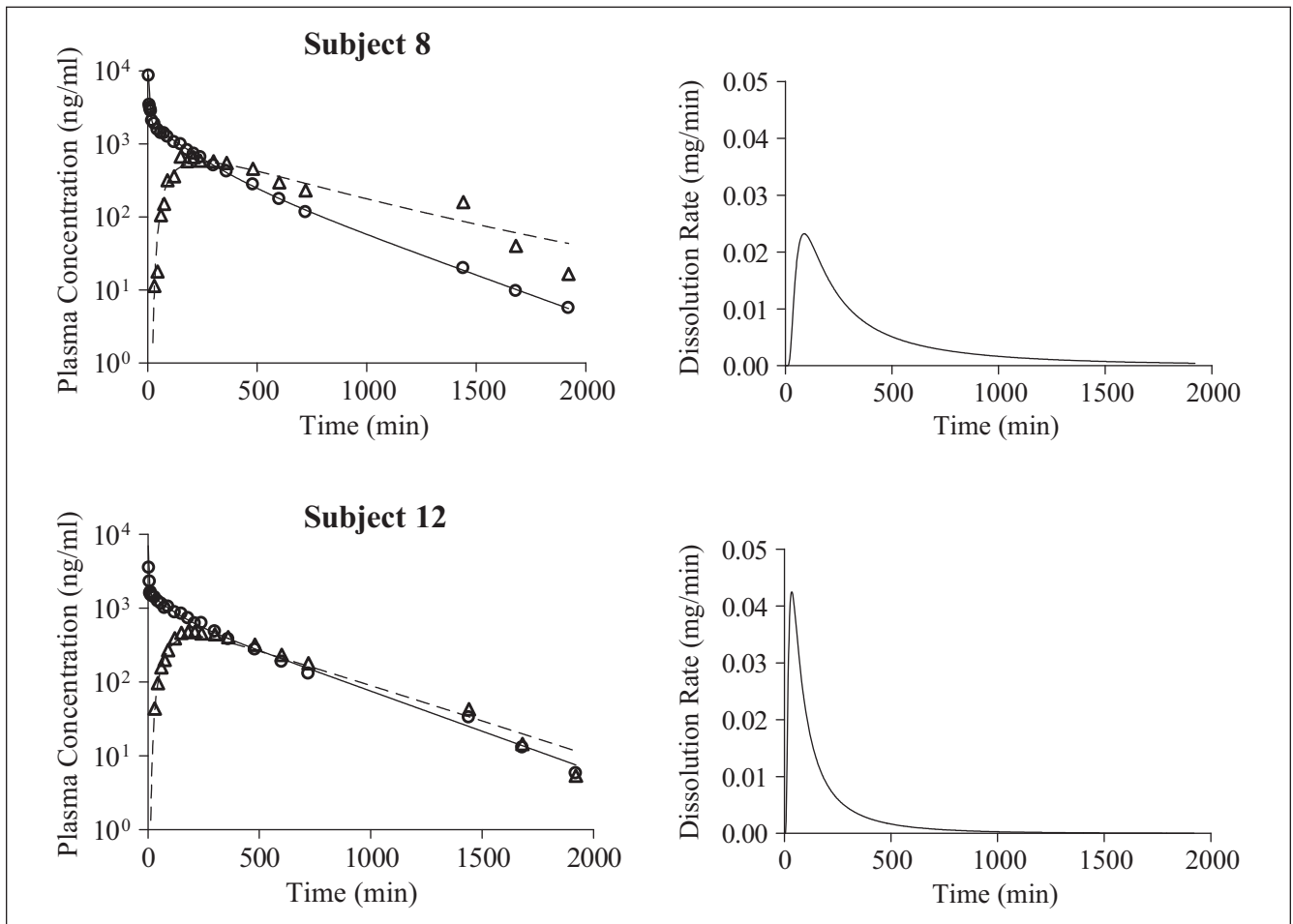


Figure 2. Predicted (lines) and measured (symbols) plasma versus time data for 2 subjects treated with the sustained-release drug, together with the corresponding predicted dissolution/transit functions from the IG/MAT model. The individual subject results (conditional means) are as follows: subject 8:  $MDT = 554$  min,  $MAT = 16.2$  min,  $CV_D^2 = 2.03$ ,  $F = 87.0\%$ ,  $t_{D,max} = 88.3$  min; subject 12:  $MDT = 191$  min,  $MAT = 51.8$  min,  $CV_D^2 = 1.79$ ,  $F = 59.2\%$ ,  $t_{D,max} = 34.5$  min.

are comparable to the corresponding kinetic parameters from the sequential population analysis.

A comparison of the in vivo estimate of  $MDT$  (318 minutes; see Table II) with the in vitro  $MDT$  of 302 minutes suggests that the IG function essentially represents dissolution of the formulation as the rate-limiting input process. As expected, the in vitro intertablet variability (13%) of  $MDT$  is lower than the intersubject variability (36%). It is also not surprising that the shape of the calculated in vivo dissolution rate profile differs from that measured in vitro (shape parameter  $CV_D^2 = 1.93$  vs 3.72).

In the trapidil example, the modeling results indicate that approximately 75% of the mean input time is due to the dissolution/transit process, with 25% due to the absorption process (Table II). That the

intersubject variability in the input process (approximately 50% coefficient of variation [CV] in  $MDT$ , 150% CV in  $t_{D,max}$ , and 85% CV in  $MAT$ ) is much higher than that observed in healthy volunteers (Table I) can be explained by the effect of liver disease on the absorption process in these patients (see below). This example also illustrates that for a sampling regimen that does not sufficiently cover the terminal phase after oral administration, the present method—in contrast to conventional calculation of AUC by numerical methods—allows an estimation of both the extent and rate of bioavailability. The estimate of  $F$  is in agreement with the complete bioavailability (95% confidence limits of 90% and 122%) obtained in healthy volunteers,<sup>18</sup> as suggested by the fact that in patients with liver disease,

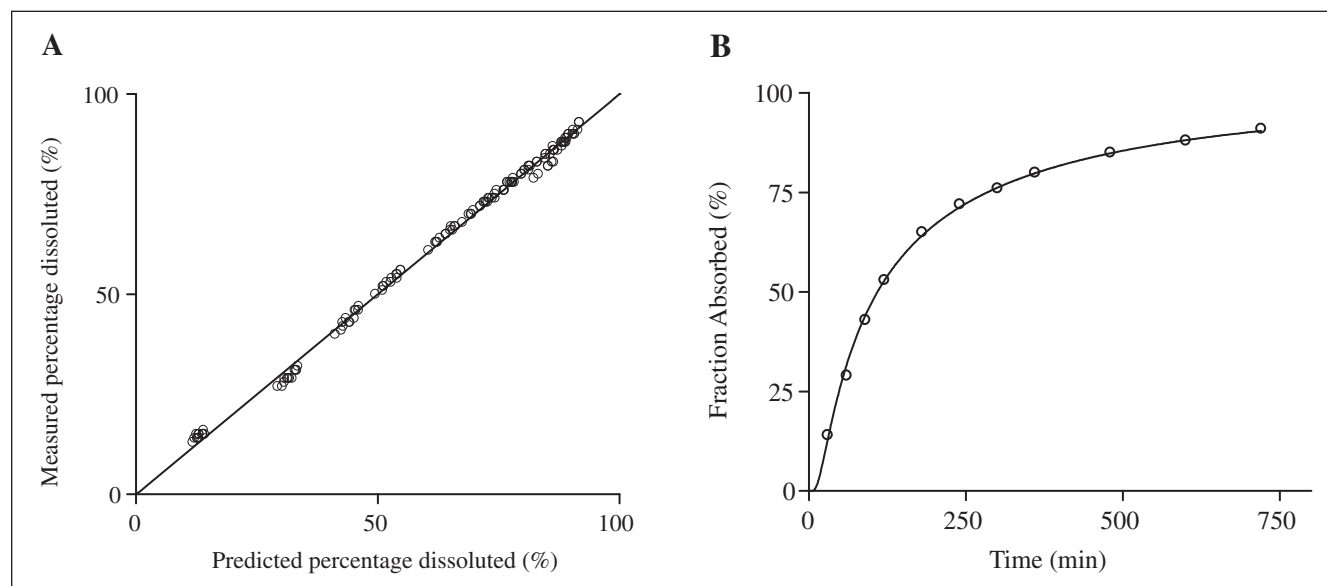


Figure 3. Analysis of in vitro dissolution profile of 12 extended-release formulations: measured data versus predicted individual concentration values (A) along with a representative example of a fitted model (B).

**Table II** Comparison of the Population Analysis of Tropicamide Oral Data Using the 2 Different Input Models

	IG/MAT Model		IG Model		
	Population Mean	Population SD	Population Mean	Population SD	
$F$ , %	90.2	31.9	$F$ , %	90.5	30.9
$MDT$ , min	100	50.4	$MIT$ , min	134	59.8
$MAT$ , min	30.6	25.9			
$CV_D^2$	1.64	2.83	$CV_I^2$	0.740	0.788
$t_{D,max}$	19.6	29.6	$t_{I,max}$	51.7	26.6
AIC	235			250	

IG, inverse Gaussian; AIC, Akaike information criterion.

bioavailability is hardly reduced (but may increase due to a reduced first-pass metabolism). That the mean input time in healthy volunteers is only about 50% of that in patients is in accordance with a delayed drug absorption process in liver disease.<sup>19</sup> In contrast to the extended-release example, there is no clear interpretation of the specific role of the components of the IG/MAT model ( $MAT$  and  $MDT$ ).

Taken together with previous applications, these examples further demonstrate the utility of the inverse Gaussian function for modeling extravascular input processes and show that the addition of a first-order absorption process improves the fit of oral data. Inverse Gaussian function models offer a more compact and flexible approach for quantifying extravascular inputs compared with commonly used

parametric models (eg, first-order absorption with lag, zero-order input, etc), at the expense of a modest increase in computational complexity. This approach avoids biased parameter estimates that are likely to occur if unrealistic models are used.<sup>3</sup> Compared with nonparametric deconvolution methods, the approach is numerically stable and allows for direct estimation of and inferences based on absorption process parameters, but as implemented, it limits the form of the input function (for extension, see Verotta<sup>1</sup>). Model building using the inverse Gaussian function can now be performed conveniently as part of a population as well as an individual subject analysis using the ADAPT software (Version 5), which includes in its library the inverse Gaussian function models presented herein.<sup>17</sup>

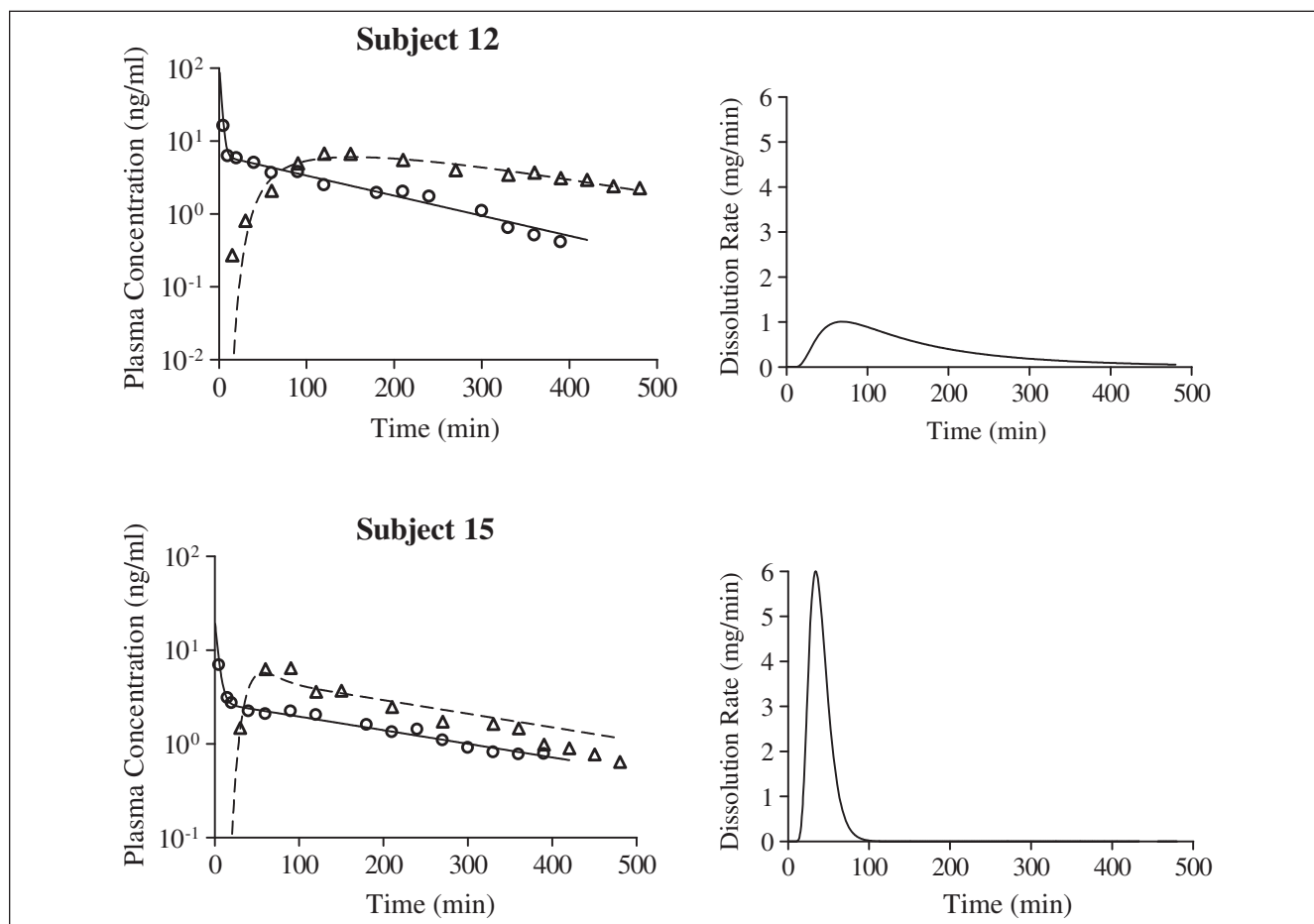


Figure 4. Predicted (lines) and measured (symbols) plasma versus time data for 2 subjects treated with trapidil, together with the corresponding predicted dissolution/transit functions from the IG/MAT model. The individual subject results (conditional means) are as follows: subject 12: MDT = 184 min, MAT = 11.2 min,  $CV_D^2 = 0.765$ ,  $F = 92.3\%$ ,  $t_{D,max} = 69.7$  min; subject 15: MDT = 40.0 min, MAT = 12.1 min,  $CV_D^2 = 0.109$ ,  $F = 87.8\%$ ,  $t_{D,max} = 34.0$  min.

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